

Image Analysis in Neuroinformatics

Removal of Artifacts

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Characterization of Arfitacts

Characterization of Artifacts I

Random noise

 $p_{\eta}(\eta)$

Mean

•Pdf

$$\mu_{\eta} = E[\eta] = \int_{-\infty}^{\infty} \eta p_{\eta}(\eta) \, \delta\eta$$

Variance

$$\sigma_{\eta}^{2} = E[(\eta - \mu_{\eta})^{2}] = \int_{-\infty}^{\infty} (\eta - \mu_{\eta})^{2} p_{\eta}(\eta) \,\delta\eta$$
$$\sigma_{\eta}^{2} = E[\eta^{2}] - E[\eta]^{2}$$



Image



Detected image

Image frame

Noise (typically additive)

$$E[g] = \mu_g = \mu_f + \mu_\eta$$
$$E[(g - \mu_g)^2] = \sigma_g^2^2 = \sigma_f^2^2 + \sigma_\eta^2$$

Characterization of Artifacts III

- Statistical expectation
 - Estimated mean (M observations)

$$\mu_f(x_1, y_1) = \lim_{M \to \infty} \frac{1}{M} \sum_{k=1}^M f_k(x_1, y_1)$$

Autocorrelation function

 $r_f(x_1, x_1 + \alpha, y_1, y_1 + \beta) = E[f^*(x_1, y_1)f(x_1 + \alpha, y_1 + \beta)]$

$$\check{\mathbf{r}}(\alpha,\beta) = \frac{1}{XY} \sum_{x_1=0}^{X} \sum_{y_1=0}^{Y} f^*(x_1,y_1) f(x_1 + \alpha,y_1 + \beta)$$

 $r_f(0,0) \Rightarrow energy$

Characterization of Artifacts IV

• Stationarity in strict sense

Statistics not affected by a shift in time or space

• Stationarity in wide sense

Constant mean and autocorrelation depends only upon the shift in time or space

 $\mu_f(k) = \mu_f$ $r_f(t_1, t_1 + \tau) \Rightarrow r_f(\tau)$ $r_f(x_1, x_1 + \alpha, y_1, y_1 + \beta) \Rightarrow r_f(\alpha, \beta)$

Characterization of Artifacts V

Ergodicity

- Temporal statistics independent of the sample observed
- Statistics may be computed from a single observation



Gaussian noise l

- Completely specified by the mean and variance
- Important i central limit teorem
- Termal noise 📫 electronic components

$$p(x) = \frac{1}{\sqrt{2\pi\sigma_x^2}} e^{-\left(\frac{(x-\mu_x)^2}{2\sigma_x^2}\right)}$$







• Errors in linear prediction





Poisson noise

- Quantum noise, photon noise
- Signal dependant
- Systems in low-light conditions

$$p(k) = \frac{\mu^k}{k!} e^{-\mu}$$

Degraded image

0.35

15

20

25

30

10

 $p(g_0(m,n)|f(m,n),\lambda) = \frac{[\lambda f(m,n)]^{g_0(m,n)}}{g_0(m,n)!}e^{-\lambda f(m,n)}$



Other types of noise and artifact

Structured noise

- Power line interference
- Grid artifact 📃
- parallel periodic strips
- Surgical implants

Physiological interference

- Effect of breathing
- Cardiovascular activity

Others

- Salt and pepper noise
- Shot noise

Matrix Representation of Images

Matrix Representation of Images

- $F = \{F(m,n), m = 0...M-I, n + 0...N-I\}$
- Non-negativity and Upperbound Constraint
 Fmin <= F(m,n) <= Fmax
- Finite energy
 - $\varepsilon F = \Sigma \Sigma F2(m,n) \leq = Emax$
- Smoothness
 - $F(m,n) mean(Fnbd(m,n)) \le S$

Vectorization

- Useful representation prior to application of transformation, estimation, optimization
 - F = [I 2
 - 3 4]
 - Row ordering
 - f = [1 2 3 4]^T
 - Column ordering
 - $f = [1 \ 3 \ 2 \ 4]^T$
 - F is MxN, f is MNx1

Some definitions

- Energy \in = fTf = Tr[ffT]
- Mean $\mu = E[f]$
- Covariance $\sigma = E[(f \mu)(f \mu)T] = E[ffT] \mu\mu T$
- Auto Correlation or scatter matrix $\Phi = E[ffT]$
- For 2 images f,g we can define:
- Uncorrelatedness, Orthogonality, Statistical Independence (look up last week's slides)

Matrix Representation of Transforms I

- ID Transforms
- A signal may be represented as a linear combination of orthogonal basis functions

$$f(t) = \sum_{k=0}^{\infty} a_k \varphi_k(t)$$

$$\int_{t_0}^{t_0+T} \varphi_k(t)\varphi_l^*(t)dt = 1, k = l, 0, otherwise$$

$$a_k = \int_{t_0}^{t_0+T} f(t) \varphi_k^*(t)$$

Matrix Representation of Transforms II

- ID Transforms
- The set {ak} represents a 'Transform space'
- If a ID signal is sampled at N points, the transform may be represented as matrix multiplication

$$F = Lf$$

$$f = L * f$$

$$L(k,n) = \varphi_k(n)$$

Matrix Representation of Transforms III

- 2D Transforms
- For an NxN image f(m,n) and its transform
 F(k,l) are related by

$$F(k,l) = \frac{1}{N} \sum_{n=0}^{N-1} \sum_{m=0}^{N-1} f(m,n) \varphi(m,n,k,l)$$

$$f(m,n) = \frac{1}{N} \sum_{k=0}^{N-1} \sum_{l=0}^{N-1} F(k,l) \psi(m,n,k,l)$$

φ(m,n,k,l) is the forward kernel and
Ψ(m,n,k,l) is the inverse kernel

2D Transforms I

- If φ(m,n,k,l) = φl(m,n) φ2(k,l), φ is said to be separable
- If $\phi I(m,n) = \phi 2(m,n)$, it is said to be symmetric
- If φ is symmetric and separable, the 2D transform can be computed as 2 ID transforms sequentially

$$F_{1}(m,l) = \sum_{n=0}^{N-1} f(m,n)\varphi(n,l)$$
$$F(k,l) = \sum_{m=0}^{N-1} F_{1}(m,l)\varphi(m,k)$$

2D Transforms II

Example of separable, symmetric kernels:2D DFT

$$\varphi(m,n,k,l) = \exp\left[-j\frac{2\pi}{N}(mk+nl)\right]$$
$$\varphi(m,n,k,l) = \exp\left[-j\frac{2\pi}{N}mk\right]\exp\left[-j\frac{2\pi}{N}nl\right]$$

 f is the NxN image,W is a symmetric NxN matrix and F is the NxN 2D DFT

$$W(k,m) = \exp\left[-j\frac{2\pi}{N}km\right]$$

Matrix Representation of Convolutions I

ID Convolution with Causal IIR filter

$$g(n) = \sum_{\alpha=0}^{n} f(\alpha)h(n-\alpha)$$

• Can be represented in matrix form as

$$\begin{pmatrix} g(0) \\ g(1) \\ \vdots \\ g(N) \end{pmatrix} = \begin{pmatrix} h(0) & 0 & \cdots & 0 \\ h(1) & h(0) & \ddots & 0 \\ \vdots & \vdots & \ddots & \vdots \\ h(N) & h(N-1) & \cdots & h(0) \end{pmatrix} \begin{pmatrix} f(0) \\ f(1) \\ \vdots \\ f(N) \end{pmatrix}$$

Matrix Representation of Convolutions II

ID Convolution with Non-Causal FIR filter

$$g(n) = \sum_{\alpha=0}^{M} f(\alpha + n - \frac{M}{2})h(\frac{M}{2} - \alpha)$$

Can be represented in matrix form as



Matrix Representation of Convolutions III

 Periodic or circular convolution for finite, periodic f(n) and h(n)

$$g(n) = \sum_{\alpha=0}^{n} f(\alpha)h([n-\alpha] \mod N)$$

- Circular convolution of 2 signals of duration N is of length N (obtained also by IDFT of product of 2 DFTs)
- Linear convolution of 2 signals of duration N is of length 2N-1
- Circular and linear convolution can be made identical by zero padding the signals to length 2N-1

Matrix Representation of Convolutions IV

• Circular convolution in matrix form

$$\begin{pmatrix} g(0) \\ g(1) \\ \vdots \\ g(N-2) \\ g(N-1) \end{pmatrix} = \begin{pmatrix} h(0) & h(N-1) & \cdots & h(2) & h(1) \\ h(1) & h(0) & \ddots & h(3) & h(2) \\ \vdots & \vdots & \ddots & \vdots & \vdots \\ h(N-2) & h(N-1) & \ddots & h(0) & h(N-1) \\ h(N-1) & h(N-2) & \cdots & h(1) & h(0) \end{pmatrix} \begin{pmatrix} f(0) \\ f(1) \\ \vdots \\ f(N-2) \\ f(N-1) \end{pmatrix}$$

• This is called a circulant matrix.

Important property: Diagonalized by DFT

2D Convolution I

2D LSI convolution

$$g(m,n) = \sum_{\alpha=0}^{M-1} \sum_{\beta=0}^{N-1} f(\alpha,\beta)h(m-\alpha,n-\beta)$$

2D Circular convolution

$$g(m,n) = \sum_{\alpha=0}^{M-1} \sum_{\beta=0}^{N-1} f(\alpha,\beta)h([m-\alpha] \mod M, [n-\beta] \mod N)$$

2D Convolution II

• Matrix representation

$$g = hf$$

- Representation of **h** as block circulant matrix
- Insert eqn 3.102 (pg. 221)
- Submatrices \mathbf{h}_{m} are given by
- Insert eqn. 3.103 (pg. 221)
- Each h_m is circulant and h is block circulant

Denoising Techniques

Mutliframe Averaging I

- Gated ensemble averaging
- Successive frames which are gated (phase locked) to a 'physiological state' in a recurring cycle are averaged to remove additive noise
- 'Recurring physiological state' is not very clearly defined as far as the brain is concerned!

 $g = f + \eta$

• Law of large numbers suggests

 $\sigma(g) = I/sqrt(N) \sigma(\eta)$

Multiframe Averaging II

5 zero mean Gaussian noise (σ =5) frames were added to an anatomical image and averaged



Spatial Domain Local Statistics Filters

- Cannot rely on ensemble of images to obtain properties of the image
- A (spatially) moving window is used to gather local statistics
- If the statistic is a linear combination of intensities in the nbd, it can be expressed as a LSI convolution



Mean Filter

- A local neighbourhood of each pixel is considered as an ensemble
- Each pixel is substituted by its local spatial average



Oversmoothing may be avoided by selectively applying to 'non edge' pixels. This however, makes the filter non linear

Median Filter

- Each pixel is replaced by the median of its local neighborhood
- Uselful to remove outliers in the histogram (eg. Impulse noise)



Order Statistics Filters

- A class of non linear filters
- The pixels in the nbd are ordered by intensity
- i-th entry is the output of the i-th order statistic filter
- Eg. Ist entry is the min-filter
- 2nd entry is the max-filter
- Middle entry is the median-filter
- α trimmed mean filter: α percent of the top and bottom of the list are rejected and the mean of the rest is chosen



Procedure

- 2D Fourier transform of the image, padding the image with 0
 F(k,l)
 - Design or select the appropriate 2D filter transfer function
 H(k,l)
- Obtain the filtered image in Fourier Domain (center or fold)
 G(k,l)=H(k,l)F(k,l)
- Inverse Fourier Fourier Transform of G(k,l), (unfold)
 G(m,n)
- Trim the resulting image g(m,n), if it was zero-padded

Ideal lowpass filter

D0 = 20

$$H(u,v) = \begin{cases} 1, & D(k,l) < D_0 \\ 0, & otherwise \end{cases} \quad D(k,l) = \sqrt{k^2 + l^2} \end{cases}$$







Removal of high-frequency noise



10 20 30 40 50 60

Removal of peridodic artifacts







Wiener filtering: equations II

$$y = \hat{f} = h_{opt}^{H} g = P^{H} R_{g}^{-1} g \quad y = \hat{f}_{book} = h_{opt}^{H} g = R_{f} (R_{f} + R_{n})^{-1} g$$

Mse:

$$\xi_{min} = P_f - P^H R_g^{-1} P$$

Fourier domain:

$$\widetilde{F(k,l)} = \left[\frac{1}{1 + \frac{S_{\eta(k,l)}}{S_{f(k,l)}}}\right] G(k,l)$$

Wiener filtering: more aplications





Removal of noise with Wiener filtering

Gaussian noise





End of the presentation

Questions round